

## Current Trends and Recent Advances in Surface Texture of Endosseous Dental Implants: An Overview

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### Abstract

This review article describes about the various surface treatments or modifications of the dental implants. Previously dental clinicians believe that osteogenic cells did not respond to the changes in the Nano structure of the dental implant surface but recent studies have shown that Osteogenic cells respond to the surface modifications or various surface modifications<sup>1</sup>. This review article describes about the Titanium dioxide Nano tube arrangement, functional peptide coatings, fluoride treatment, calcium phosphorus application, UV photo functionalization. Various studies have shown that these surface treatments increase the dental implant survival rate to 95%.

**Keywords:** Surface texture, implants, endosseous, current trends.

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### INTRODUCTION

Osseointegration is an essentially demarcation response to a foreign body titanium which is an immune driven type 4 hypersensitivity reaction. Osseointegration plays a key role in success of dental implants [1]. Surface is important for better osseointegration of the dental implant. Titanium is a best material of choice for dental implants because of its properties like excellent biocompatibility, corrosion resistance, high strength, low modulus of elasticity and easy machinability [2]. Surface modifications of dental implant improve the wettability of the implant surface so that it improves the cell to implant adhesion, cell proliferation and osseointegration which leads to the better secondary

stability of the dental implant. Recently many studies have been carried out on surface treatment commercial pure Titanium to improve the osseointegration. Initially after implant placement stability of the dental implant occurs with the friction this is called as primary stability. Primary stability decreases subsequently to implant insertion while secondary stability increases. After 2-3 weeks, the implant stability is the lowest in a phase called implant stability dip. This secondary stability occurs with the osseointegration after placement of the dental implant so for an implant success not only the primary stability but also the secondary stability also important features [3] (Figure 1).

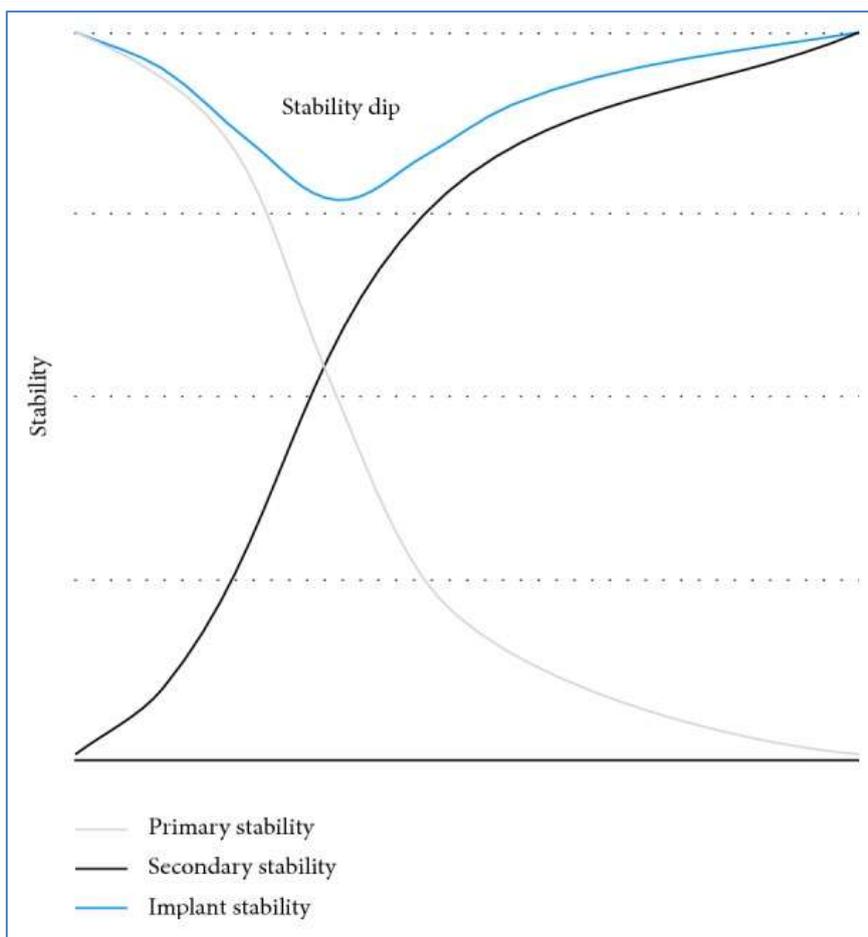


Fig-1: Figure Showing Primary Stability & Secondary Stability Post Implant Placement

**Need for implant surface treatment [2]**

To increase the surface area of the dental implant, to bring better bonding between implant surface and surrounding bone, to increase surface roughness of the dental implant, to make them more passive, to remove the surface contamination

According to Albrektsson & wennerberg commercially available implants have been categorised into four types

1. Smooth (sa<0.5micro meters)
2. Minimally rough (sa 0.5-1)
3. Moderately rough (sa1-2)
4. Rough (sa>2)

**Table-1: Different surface treatments classification [3]**

• Subtractive treatments	• Additive treatments
Machined	Anodization
• Sandblasted	• Fluoride surface treatment
• Acid-etched surface	• plasma spraying Ti Hydroxyapatite (HA).
• Dual acid-etching	Coating sol-gel
• Sandblasted and acid etched surface (SLA)	• Sputter deposition
• Laser treatment	• Electrophoretic deposition
	• Biomimetic precipitation
	• Drugs incorporated

**Machined surface (turned surface)[4]**

The presence of crease, crinkle, and splotch by the device used for the manufacturing on the surfaces of machined implants provides mechanical interlocking. The morphology of machined implants encourages the proliferation of osteoblastic cells into the grooves and

roughened surfaces on the dental implant, which is a disadvantage. The machined implant surface is considered to be minimally rough. Machined implant surfaces have SA values of 0.3-1.0 µm. This feature requires a longer waiting time between surgery and implant loading.

**Sand blasted surface treatment [4]**

Maximum surface roughness required to achieve affective biological response is 1.5 micrometers. In this technique implant surface blasted with ceramic particles. Surface roughness depends on the size of the ceramic particles. Other materials that are used to sand blasting the implant surface are aluminum oxide, titanium dioxide, silicon dioxide. These particles accelerate the osseointegration process when releases into the surrounding physiological environment and decreases the corrosion resistance [5, 6].

**Alkaline etching [7]**

Procedure: treatment of titanium with 4-5M NaOH at 600°C for 24 hrs. This procedure results in formation of sodium titanate of 1micrometer thickness with irregular topography, if this procedure is carried out after acid etching results in increased porosity.

**Surface treatment by acid etching**

Acids that are used to etch the dental implant surface are HCL, H<sub>2</sub>SO<sub>4</sub>, HNO<sub>3</sub>, and HF. In this procedure implant surface should be etched by immersing in to the mixture of concentrated HCL and H<sub>2</sub>SO<sub>4</sub> at above 100°C. This procedure is called as dual acid etching procedure [8]. It creates microoughned surface for accelerated osseointegration and it increases the osteoconductive process by attachment of fibrin, and osteogenic cells leading to bone formation on the implant microughned surface. Another approach is fluoride treatment which leads to formation of TiF<sub>4</sub> this accelerates the osseointegration process [7].

**SLA (sand blasted and acid etched surface)**

It is done by process of sand blasting with 250-500 micrometers size ceramic particles and by etching the implant surface with HCl and H<sub>2</sub>SO<sub>4</sub>, this procedure results a new hydrophilic surface calls SLA active. This SLA active creates a chemically active surface. To this anions which are taken from acids such as fluoride ions also added. Most of the studies have shown that SLA treated implants creates a greater bone contact and stability at early healing phase of 6 weeks. Laser treatment: the laser ablation develops micro roughness on dental implant surface which increases the osseointegration, resistance to corrosion and a large quality of purity with a definitive roughness and compact oxide layer [7-9].

**Additive treatments**

Anodization: This procedure is carried out at high voltage in strong acids like H<sub>3</sub>PO<sub>4</sub>, HNO<sub>3</sub>, H<sub>2</sub>SO<sub>4</sub>, HF resulting in crystallization of surface. It leads to thickening of oxide layer to more than 1000 nm on implant surface. This process accelerates the osseointegration more than that of machined surfaces [10].

Fluoride treatment: Ti surface is very sensible to fluoride ions and it forms TiF which is soluble in nature. This process increases the osteoblastic differentiation and osseointegration. fluoride ion treated implants also had a greater push out forces and showed a significantly more advanced torque removal forces in many studies [9].

**Roughening of implant surface by plasma spraying**

The advantage of this technique is that these layers give implants a porous surface making easy for the bone to penetrate easily. The implant rough surface within the range of 50-400 micro meters. Titanium and calcium phosphate can be added by plasma spraying technique [10].

Titanium plasma spraying: titanium plasma spraying was introduced approx 35 years back. Primarily in 1970, Hahn & Palich described micro porous nature of surface of orthopaedic implants, which was later attempted in dental implants by Schroeder et al. this procedure includes heating titanium to plasma form and spray this plasma on implant surface which can increase the apertures on implant surface by six times (30 to 50 µm deep), thus enhancing micro retention. The surface area of implant after plasma-spray is around 3 times that of a machined surface [11].

**HA plasma spraying**

Hydroxy apatite is one of the materials that forms strong bond between titanium implant and bone, it improves the chemical and mechanical properties and increases the corrosion resistance. Plasma-spraying is a technique in which hydroxyapatite (HA) ceramic particles are injected into a plasma torch at high temperature and projected on to the surface of the titanium dental implant where they condense and fuse together, forming a film. Plasma-sprayed coatings can be deposited with a thickness ranging from a few micro meters to a few milli meters. When using this method in order to obtain mechanical retention of the coating, the surface of the titanium dental implant must be roughened by means of grit blasting [12]. The plasma-spraying method has disadvantages, however, such as the porosity of the coating and residual stress at the substrate/coating interface, as well as drastic changes in the composition and crystallinity of the initial calcium phosphate powder. Several calcium phosphate phases have been observed in plasma-sprayed HA coatings such as tricalcium phosphates, tetracalcium phosphate calcium oxide and amorphous calcium phosphate (ACP). The main disadvantage of this technique is delamination of the hydroxyl apatite layer [13]. Sol gel coated implants: this technique is straight forward and inexpensive. This technique includes homologous chemical distribution on the implant surface. The main advantage of this technique is increased toughness when compare with bioactive ceramics, biological acceptability which leads to early bone formation during healing phase and mechanical strength [13].

**Sputter deposition:** This is a process in which high energy ions are discharged in a vacuum chamber to change the surface texture of a titanium implant surface [14].

**Radiofrequency sputtering:** This process includes the formation of thin film of calcium phosphate coatings on dental implants. It forms strong adhesive link between titanium and calcium phosphate [13].

**Magnetron sputtering:** This process includes formation of the TiO<sub>2</sub> layer at the bone and implant surface which establishes the strong bond between titanium and hydroxyl apatite layer [13].

**Biomimetic calcium phosphate coatings:** This process implant surface will have plasma sprayed hydroxyl apatite coating which is inspired by the natural process of ion mineralisation and this contains modification like condensation of the calcium phosphate apatite crystals on the surface of the dental implants. These biomimetic coatings are more soluble in physiological fluids and resorbable by osteoclastic cells [15].

**Biologically active drug incorporated dental implants:** surface treatment with osteogenic and antiresorptive drugs like bisphosphonates improves the osseointegration [16].

### **Bisphosphonates**

Bisphosphonates like pamidronate and zoledronate escalates the bone contact area but the major disadvantage of this technique will be present in the grafting and slow discharge of drug on the surface of titanium implant [16].

### **Simvastatin**

Increases the release of bone morphogenic protein 2 mRNA which accelerates the bone formation. Most of the studies have shown that surface treatment with simvastatin increases the bone mineral density around the dental implant [16].

### **Antibiotic coating**

Gentamycin with hydroxyapatite coating on dental implant surface will act like prophylactic agent around the implant and it reduces the surgical site infection.

Tetracycline-HCL surface treatment can be used as practical and efficient chemical method for decontamination and detoxification of harmed surface of implants [17].

## **CONCLUSION**

Previously success rate of dental implants were more common. To overcome these complications and to increase the success of the dental implants various surface modifications are introduced and still research

is going on the future trends like biomimetic surface coatings and drug induced surface coatings to improve the quality of the dental implants.

## **REFERENCES**

1. Fouziya, B., Uthappa, M. A., Amara, D., Tom, N., Byrappa, S., & Sunny, K. (2016). Surface modifications of titanium implants—The new, the old, and the never heard of options. *Journal of Advanced Clinical and Research Insights*, 3(6), 215-219.
2. Carlsson, L. V., Albrektsson, T., & Berman, C. (1989). Bone response to plasma-cleaned titanium implants. *International Journal of Oral & Maxillofacial Implants*, 4(3).
3. Wennerberg, A., Bolind, P., & Albrektsson, T. (1991). Glow-discharge pretreated implants combined with temporary bone tissue ischemia. *Swedish dental journal*, 15(2), 95-101.
4. Cochran, D. L., Schenk, R. K., Lussi, A., Higginbottom, F. L., & Buser, D. (1998). Bone response to unloaded and loaded titanium implants with a sandblasted and acid-etched surface: A histometric study in the canine mandible. *Journal of Biomedical Materials Research: An Official Journal of The Society for Biomaterials, The Japanese Society for Biomaterials, and the Australian Society for Biomaterials*, 40(1), 1-11.
5. Urban, R. M., Jacobs, J. J., Tomlinson, M. J., Gavrilovic, J., Black, J., & Peoc'h, M. (2000). Dissemination of wear particles to the liver, spleen, and abdominal lymph nodes of patients with hip or knee replacement. *JBJS*, 82(4), 457.
6. Browne, M., & Gregson, P. J. (2000). Effect of mechanical surface pretreatment on metal ion release. *Biomaterials*, 21(4), 385-392.
7. Martini, D., Fini, M., Franchi, M., De Pasquale, V., Bacchelli, B., Gamberini, M., ... & Raspanti, M. (2003). Detachment of titanium and fluorohydroxyapatite particles in unloaded endosseous implants. *Biomaterials*, 24(7), 1309-1316.
8. Cho, S. A., & Park, K. T. (2003). The removal torque of titanium screw inserted in rabbit tibia treated by dual acid etching. *Biomaterials*, 24(20), 3611-3617.
9. Park, J. Y., & Davies, J. E. (2000). Red blood cell and platelet interactions with titanium implant surfaces. *Clinical oral implants research*, 11(6), 530-539.
10. Trisi, P., Lazzara, R., Rebaudi, A., Rao, W., Testori, T., & Porter, S. S. (2003). Bone-implant contact on machined and dual acid-etched surfaces after 2 months of healing in the human maxilla. *Journal of periodontology*, 74(7), 945-956.
11. Trisi, P., Marcato, C., & Todisco, M. (2003). Bone-to-implant apposition with machined and MTX microtextured implant surfaces in human

- sinus grafts. *International Journal of Periodontics & Restorative Dentistry*, 23(5).
12. Cochran, D. L., Buser, D., Ten Bruggenkate, C. M., Weingart, D., Taylor, T. M., Bernard, J. P., ... & Simpson, J. P. (2002). The use of reduced healing times on ITI® implants with a sandblasted and acid- etched (SLA) surface: Early results from clinical trials on ITI® SLA implants. *Clinical oral implants research*, 13(2), 144-153.
  13. Novaes Jr, A. B., Papalexiou, V., Grisi, M. F., Souza, S. S., Taba Jr, M., & Kajiwarra, J. K. (2004). Influence of implant microstructure on the osseointegration of immediate implants placed in periodontally infected sites: a histomorphometric study in dogs. *Clinical Oral Implants Research*, 15(1), 34-43.
  14. Taba Jr, M., Novaes Jr, A. B., Souza, S. L., Grisi, M. F., Palioto, D. B., & Pardini, L. C. (2003). Radiographic evaluation of dental implants with different surface treatments: an experimental study in dogs. *Implant dentistry*, 12(3), 252-258.
  15. Ong, J. L., Carnes, D. L., & Bessho, K. (2004). Evaluation of titanium plasma-sprayed and plasma-sprayed hydroxyapatite implants in vivo. *Biomaterials*, 25(19), 4601-4606.
  16. Aparicio, C., Gil, F. J., Fonseca, C., Barbosa, M., & Planell, J. A. (2003). Corrosion behaviour of commercially pure titanium shot blasted with different materials and sizes of shot particles for dental implant applications. *Biomaterials*, 24(2), 263-273.
  17. Müller, W. D., Gross, U., Fritz, T., Voigt, C., Fischer, P., Berger, G., & Lange, K. P. (2003). Evaluation of the interface between bone and titanium surfaces being blasted by aluminium oxide or bioceramic particles. *Clinical Oral Implants Research*, 14(3), 349-356.
  18. Massaro, C., Rotolo, P., De Riccardis, F., Milella, E., Napoli, A., Wieland, M., & Brunette, D. M. (2002). Comparative investigation of the surface properties of commercial titanium dental implants. Part I: chemical composition. *Journal of Materials Science: Materials in Medicine*, 13(6), 535-548.